

On chip thermal calibration with 8CB liquid crystal of micro-thermal device for biological applications.

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A micro sensor integrated on a micro-thermal device for bio-experiments requires affordable, rapid and accurate thermal calibration. However, there has been no way to make thermal calibration directly under the microscope. This was the limitations in making numbers of bioexperiments with micro thermal devices. We present in this paper an inexpensive, fast and accurate way to realise such thermal calibration directly under the microscope. We used a thermotropic liquid crystal: the 4-n-octyl-4-cyanobiphenyl (8CB) in order to reach the 313 K isothermal phase change on the device. Coupled with FEA simulations, we proved that this method enables us to make easy and accurate thermal calibration of micro-thermal device for biological application.

Rapid switching and measurement of the temperature in a liquid are of paramount importance for real time observation of activities of biomolecules such as protein folding-unfolding or enzymatic reactions.^{1, 2} This rapid switching must be achieved under the microscope. Controlling the temperature of small liquid volume is the most promising method. Due to the small heat energy required for the temperature control, this realises fast response speed³ and avoids the defocusing problem in conventional bulk heating device¹.

There are several methods to achieve this, such as heating a small liquid volume with a laser beam.⁴ However, this may damage the observing biomaterials and a laser itself cannot be integrated on the microchip. The most convenient and widely applicable way is to fabricate a heater and a thermosensor on a glass plate at a microscopic scale.^{1, 5, 6} For those thermosensors on a microchip, rapid and accurate thermal calibration is inevitable. The conventional way for such calibration consists in immersing whole chip into hot water or an oven, however, these methods are time consuming and often endanger the electric circuit.

Recently, calibration using light emitting particles such as Rhodamine B has been reported.^{4, 7} However, this method is not enough accurate due to photo bleaching. Scanning thermal microscopie (SThM) offers a very accurate calibration means.^{8, 9} It

consists of an AFM used as a platform with a temperature sensing probe, most of the time a very small thermocouple. Unfortunately, this kind of measure is not already fully and easily available and is difficult to achieve. The use of a IR camera presents the advantage of being indirect measurement.¹⁰ Hence, the microthermal device does not need to be modified or combined with other equipments. Nevertheless, it can measure the thermal map only at the surface of the device and only works without water. Therefore, it doesn't match the requirements for biological experiments. Some other ways to calibrate micro thermo device can be used, such as transient thermo-reflectance.¹¹ This can be realised considering that the surface reflectivity of the heater, for example, is linearly proportional to the change in its surface temperature within a wide but finite temperature range. This calibration requires expensive and very fast equipments.

Therefore, a reliable and affordable method for calibrating a thermosensor on a chip under the microscope is required. However, this kind of calibration method has not been established yet due to the difficulty to measure the temperature in small area on a microdevice.

We propose a method using 8CB liquid crystal that we can use directly under a microscope without any modification of the microthermal device. We also demonstrate this method on a microthermal device which we have manufactured for biological applications. This calibration process can be extended to other onchip micro thermal sensors.

Liquid crystal

The use of liquid crystal for nondestructive testing has been referenced at early stage.¹² Previous researches have mainly used liquid crystal properties for real time temperature measurement of electronics device, using a camera with image processing.¹³

For the thermal calibration process, we have chosen to use a thermotropic liquid crystal: the 4-n-octyl-4-cyanobiphenyl (8CB, Fig. 1). The phases sequence of bulk 8CB on increasing temperature is crystal (X), smectic A (SmAd), nematic (N) and isotropic (I) with the following transition temperatures: $T_{XSmA}=294.5$ K, $T_{NSmA}=306.3$ K and $T_{NI}=313$ K (Fig. 1).

A recent calorimetry study led at several thermal rate and by the use of various kind of calorimeters (differential scanning calorimetry and modulation calorimetry) has shown the nature of the order of the 8CB phase transitions.¹⁴ The first transition X-

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SmA is first order with a strong enthalpy of transition. The second order SmA-N transition is characterized by a weak enthalpy of transition and presents the following character. In presence of disorder or impurities which can be present in various real materials (porous materials, dispersion of aerosols) this transition is suppressed and is replaced by the gradual occurrence of short range smectic phase^{15, 16}. The N-I transition has been recognized to be pure first order transition.¹⁴ The enthalpy of transition is weak and can easily be understood. Indeed, the Nematic phase is identified by a microscopic orientation of the molecules along one direction which defined an orientational order parameter. The reorganization of the molecules is rather weak because only one order is lost, by heating to the isotropic phase and involves a small difference of free energy between the two phases.

Within the framework of micro thermal calibration, we focus on this last N-I transition which shows keys points. The Nematic phase transits at the isothermal temperature of 313 K which is close to the room temperature, and the transition can be remarkably identified by the use of microscopy techniques (conventional and polarized microscopy) due to the change of textures between the two phases.

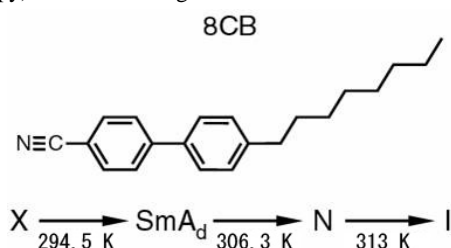


Fig. 1 8CB representation and its different phase transition temperature (X is the crystalline, SmA_d the smectic phase, N the nematic phase and I the isotropic phase)

Indeed, in a planar cell, the modification of the textures between the two phases is completely different. Without any specific anchoring selected, the Nematic phase presents some domains where it is observed some birefringence (black and white domains under polarized microscope) with texture organized around point disclinations, disclination lines and inversion walls. On the other hand, the isotropic phase at higher temperatures appears then on dark under polarized light, as it can be observed for the case of a simple liquid.

Proposed micro thermal device

We have manufactured a micro thermal device for biological applications to demonstrate the proposed calibration method (Fig. 2). This device consists in a micro heater and a thermal sensor, both manufactured on quartz wafer. The micro heater is a 2 μm wide platinum micro wire. The thermal sensor is a Pt-Cr thin film thermocouple (TFTC) with a hot junction area of 2.5x2.5 μm².¹⁷

The device manufacturing process consists of sputtering, lithographic and reactive ion etching (RIE). First titanium-platinum-SiO₂ layers are sputtered on the wafer. The titanium layer is used as an adhesive layer for the platinum. The platinum layer was patterned by RIE with a S18-05 photo resist mask. When platinum patterns are ready, chromium and SiO₂ layers are

sputtered and once again lithographic and RIE processes are used to obtain the chromium patterns. At the end, a 100 nm thick layer of SiO₂ is sputtered to provide electrical insulation between the heater and the TFTC when used during biological experiments.

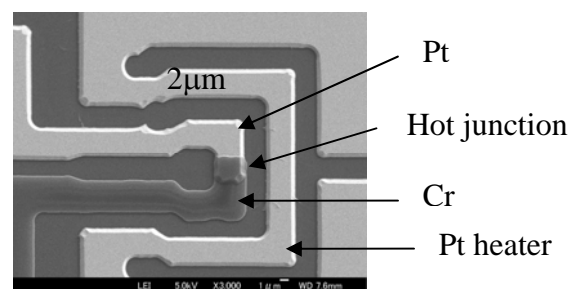


Fig. 2 SEM picture of the micro thermal device. Platinum heater and half thermocouple appear in white, chromium half thermocouple in dark.

Simulations of temperature distribution

We have simulated the thermal device behavior in steady state using finite elements analysis (FemLab 3.1). Due to consideration of symmetry, we have simulated half our device. Moreover, we have omitted the SiO₂ insulation layer on top of TFTC and heater due to its thickness (100nm). We have used planar elements to represent the heater and TFTC (thickness of 200 nm negligible) and considered that the device is initially at 297 K.

We have considered a 1 μm thick layer of 8CB trapped between the device and a cover glass, as it will be realized for experiments.

For a given input voltage, the heater provides a given amount of heat generated by Joule effect. Heat diffusion is then simulated considering the heat equation for all meshes. As the observation time length is in minutes (observation of the steady state), we have taken into account convection heating in the bulk 8CB. Finally, because of the low temperature range in the device, the radiation losses were considered negligible. Material thermal characteristics used for simulations are given as follows in Tab. 1.

We have considered only the I phase of the liquid crystal for simulation as it will be the relevant phase for the calibration and to avoid multi-phases simulations.

Table 1 Material thermal characteristics used for simulations. 8CB properties are considered in Isotropic phase.¹⁸

Material	ρ , kg.m ⁻³	C_p , J.(kg.K) ⁻¹	λ , W.(m.K) ⁻¹
Platinum	21450	133	71.6
Quartz	2203	703	1.38
8CB Iso.	870	2200	1.55

The temperature distribution is shown in Fig. 3. The nematic to isotropic change will occur at 313 K. For a small volume of Isotropic phase, simulations have shown a very low temperature variation inside the isotropic phase, i.e. it will be possible to consider that the temperature on the TFTC will be 313 K.

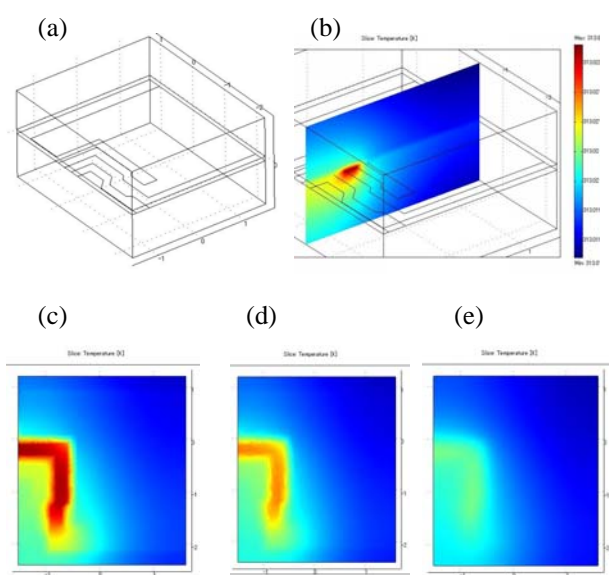


Fig. 3 Simulations results for the half device. (a) : Device in 3D, (b) : temperature distribution in a vertical plan containing the TFTC hot junction and a section of the heater. (c) : temperature distribution in an horizontal plan in the 8CB at 0.1μm, (d) 0.5μm and (e) 0.9μm above the heater and TFTC.

Calibration methodology

We observe in real time 8CB liquid crystal Nematic – Isotropic phase transition which occurs at 313 K. As it is a first order transition, the thermal sensor output recorded when the phase transition is located on it corresponds to a measured temperature of 313 K. Room temperature corresponds to null output. Considering the Pt-Cr thermo-couple linear behavior within 275 K - 375 K range, we can then obtain the thermo-couple calibration curve.

Experimental set up

We observed our micro-thermal device with a BX 51 Olympus microscope fitted with a Nikon Coolpix 4500 digital camera with two adapters (Olympus C-DMA3 and Nikon CMD).

Polybeads of 1.0 μm in diameter (Polybead@carboxylate: Polyscience, Inc.) was mixed with liquid crystal (8CB, Wako supplier, ref. 320-23511) to act as spacers. The polybeads were washed 3 times by water to substitute stock buffer (Benzene, ethenyl-, homopolymer) to pure water; 10 μL from the stock were diluted 10 times and collected by centrifugator (10000 rpm, 5 min) for each wash. After the final collection, beads were sustained in a 200 μL water. 1 μL of this beads contained water and 4 μL of 8CB were mixed at 313 K, then heated at 320 K to be easily manipulated and poured onto the thermodevice.

Liquid crystals were poured onto the microthermal device and a glass slide was placed on top of the droplet of liquid crystals so as to facilitate observation and delay evaporation. This also realise the same conditions during bioexperiments. We used a 20X objective (CF Plan: Nikon) for observation under both brightfield conditions (reflected light) and polarized (transmitted) light.

We applied different heating voltage and observed the position of the isotherm. At the same time, we recorded the output current waveform of the micro TFTC coupled with a 471Ω CMS resistor through a Keithley 428 current amplifier.

Results

The picture (a) in Fig. 4 shows the device at room temperature, i.e. at 297 K. At this temperature the liquid crystal is in Smectic phase. The device didn't receive any chemical treatment for selecting any preferential anchoring of the molecules. In this condition, it is well known that the smectic texture shows more or less regular arrays of lines under cross polarized microscopy. Another interesting point which can be underlined is the presence of the formation of smectic domains in droplet called also focal conic domains, cf. (d) in Fig. 4. Details of these focal conic domains are represented in the picture (e) Fig. 4. The droplets show faceted structure due to the anisotropic surface tension of the Smectic A phase. In the Smectic A phase, this faceting is provided by the so called focal conic domains in the form of cones of revolution.

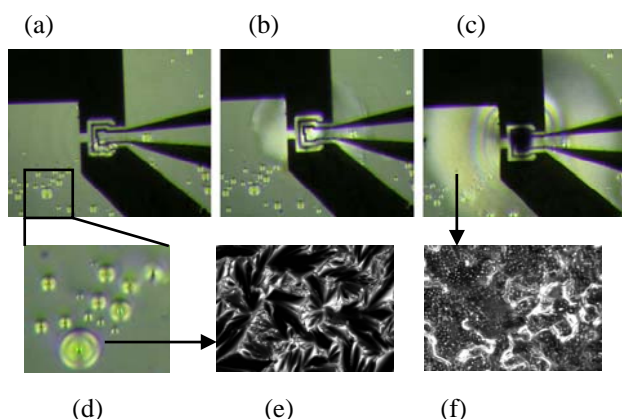


Fig. 4 Pictures taken by a BX 51 Olympus (20x and cross polarizers). Heater with (a) no input voltage, (b) 0.8V and (c) 1.2V. Smectic phase appears as gray (d, e), Nematic (f) as bright and Isotropic as dark (central dot in (c)).

The picture (b) in Fig. 4 shows the device under an applied voltage of 0.8 V. The situation is sensibly different. One can distinguish an obvious modification of both texture and turbidity of the liquid crystal close and up to the hot junction area. This area appears brighter than both Smectic A domains of the picture (a) in Fig. 4 but presents birefringence and a picture taken at higher magnification probes the existence of the 8CB Nematic phase (cf. (f) in Fig. 4) with the presence of point defects in the structure. The Nematic phase is separated of the Smectic phase by a large band of several micrometers (bright domain in (b), Fig. 4).

The picture (c) in Fig. 4 confirms the simulation presented in the Fig. 3 when a voltage of 1.2 V is applied. Under cross polarizers, one can observe a black circle which covers the totality of the microthermal heater. This phase which appears in black doesn't present by consequence any birefringence and can be identified as the Isotropic phase of the 8CB. The existence separation between the Nematic to the Isotropic phase can be easily distinguished by the differences of both birefringence and texture of the two phases. We have to notice again the advantage of this first order transition for the thermal calibration of the device since the differentiation between the Nematic and Isotropic phases is more evident than the SmA-N transition. Under such voltage of 1.2 V, the separation line between the Nematic to the Smectic phases moves. Numerous focal conic domains of the Smectic phase present in the figure 4b melt into the Nematic phase which is preponderant in this last case.

Then, by ramping the voltage by step of 0.1V, we recorded the TFTC output voltage as well as pictures from the microscope. The TFTC output as a function of the heater voltage input is illustrated in Fig. 5.

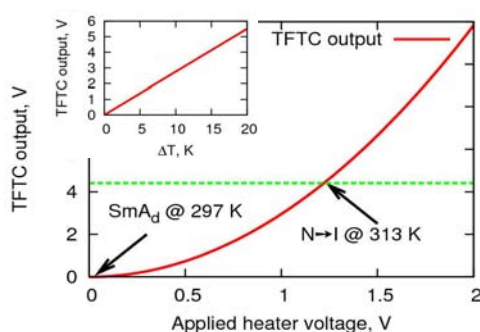


Fig. 5 TFTC output as a function of the applied heater voltage. Applied voltage step is 0.1V. The TFTC output under this heating voltage is 4.41V. In insert : TFTC output as a function of temperature difference between its hot and cold junction, ΔT .

It is then possible to consider that the TFTC is calibrated and will delivered, after amplification, $4.41/16 \approx 27.5 \cdot 10^{-2} \text{ V.K}^{-1}$. After ethanol washing using a cotton bud, the micro-thermal device is directly operational and can be used for biological applications without observation, control and acquisition set-up modification.

Conclusion

We have proposed and demonstrated a fast, easy and affordable process for steady state thermal calibration of micro thermo device directly under the microscope. Our proposed method emphasizes on the use of 8CB crystal which has proved to be an inexpensive, accurate and robust way to obtain isotherms. Our method doesn't

require any design modification of the microthermodevice, just to pour a droplet of liquid crystal on the device as we do for samples in bioexperiments. We have demonstrated its feasibility on a microthermal device equipped with a Pt-Cr thin film thermo-couple. The results indicate the feasibility of this method to general microfabricated thermal device.

Acknowledgements

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Notes and references

† Footnotes should appear here. These might include comments relevant to but not central to the matter under discussion, limited experimental and spectral data, and crystallographic data.

1. H. F. Arata, H. Noji and H. Fujita, *Applied Physics Letters*, 2006, **88**, 083902-083903.
2. H. F. Arata, Y. Rondelez, H. Noji and H. Fujita, *Anal. Chem.*, 2005, **77**, 4810-4814.
3. K. Sato, A. Hibara, M. Tokeshi, H. Hisamoto and T. Kitamori, *Advanced Drug Delivery Reviews*, 2003, **55**, 379-391.
4. M. N. Slyadnev, Y. Tanaka, M. Tokeshi and T. Kitamori, *Anal. Chem.*, 2001, **73**, 4037-4044.
5. T. Yamamoto, T. Nojima and T. Fujii, *Lab on a Chip*, 2002, **2**, 197-202.
6. G. Mihajlovic, N. M. Brunet, J. Trbovic, P. Xiong, S. von Molnar and P. B. Chase, *Applied Physics Letters*, 2004, **85**, 1060-1062.
7. H. F. Arata, P. Low, K. Ishizuka, C. Bergaud, B. Kim, H. Noji and H. Fujita, *Sensors and Actuators B-Chemical*, 2006, **117**, 339-345.
8. L. Shi and A. Majumdar, *Journal of Heat Transfer-Transactions of the Asme*, 2002, **124**, 329-337.
9. A. Majumdar, J. Lai, M. Chandrachood, O. Nakabeppu, Y. Wu and Z. Shi, *Review of Scientific Instruments*, 1995, **66**, 3584-3592.
10. L. Shi and A. Majumdar, *Microscale Thermophysical Engineering*, 2001, **5**, 251-265.
11. C. A. Paddock and G. L. Eesley, *Journal of Applied Physics*, 1986, **60**, 285-290.
12. J. L. Ferguson, *Applied Optics*, 1968, **7**, 1729-1737.
13. A. Csendes, V. Szekely and M. Rencz, *Microelectronic Engineering*, 1996, **31**, 281-290.
14. D. Sharma, J. C. MacDonald and G. S. Iannacchione, *J. Phys. Chem. B*, 2006, **110**, 16679-16684.
15. T. Bellini, L. Radzihovsky, J. Toner and N. A. Clark, *Science*, 2001, **294**, 1074-1079.
16. R. Guegan, D. Morineau, C. Loverdo, W. Beziel and M. Guendouz, *Physical Review E (Statistical, Nonlinear, and Soft Matter Physics)*, 2006, **73**, 011707-011706.
17. F. Gillot, H. F. Arata, F. O. Morin, D. Collard and H. Fujita, in *TRANSUCERS'07*, Lyon, France, 2007.
18. M. Marinelli, F. Mercuri, S. Foglietta, U. Zammit and F. Scudieri, *Physical Review E*, 1996, **54**, 1604.